# ||l-(07 |||-()7 <br> <br> Users' Library Solutions <br> <br> Users' Library Solutions Cardiac 

 Cardiac}


## INTRODUCTION

In an effort to provide continued value to it's customers, Hewlett-Packard is introducing a unique service for the HP fully programmable calculator user. This service is designed to save you time and programming effort. As users are aware, Programmable Calculators are capable of delivering tremendous problem solving potential in terms of power and flexibility, but the real genie in the bottle is program solutions. HP's introduction of the first handheld programmable calculator in 1974 immediately led to a request for program solutions - hence the beginning of the HP-65 Users' Library. In order to save HP calculator customers time, users wrote their own programs and sent them to the Library for the benefit of other program users. In a short period of time over 5,000 programs were accepted and made available. This overwhelming response indicated the value of the program library and a Users' Library was then established for the HP-67/97 users.

To extend the value of the Users' Library, Hewlett-Packard is introducing a unique service-a service designed to save you time and money. The Users' Library has collected the best programs in the most popular categories from the HP-67/97 and HP-65 Libraries. These programs have been packaged into a series of low-cost books, resulting in substantial savings for our valued HP-67/97 users.

We feel this new software service will extend the capabilities of our programmable calculators and provide a great benefit to our HP-67/97 users.

## A WORD ABOUT PROGRAM USAGE

Each program contained herein is reproduced on the standard forms used by the Users' Library. Magnetic cards are not included. The Program Description I page gives a basic description of the program. The Program Description II page provides a sample problem and the keystrokes used to solve it. The User Instructions page contains a description of the keystrokes used to solve problems in general and the options which are available to the user. The Program Listing I and Program Listing II pages list the program steps necessary to operate the calculator. The comments, listed next to the steps, describe the reason for a step or group of steps. Other pertinent information about data register contents, uses of labels and flags and the initial calculator status mode is also found on these pages. Following the directions in your HP-67 or HP-97 Owners' Handbook and Programming Guide, "Loading a Program" (page 134, HP-67; page 119, HP-97), key in the program from the Program Listing I and Program Listing II pages. A number at the top of the Program Listing indicates on which calculator the program was written (HP-67 or HP-97). If the calculator indicated differs from the calculator you will be using, consult Appendix E of your Owner's Handbook for the corresponding keycodes and keystrokes converting HP-67 to HP-97 keycodes and vice versa. No program conversion is necessary. The HP-67 and HP-97 are totally compatible, but some differences do occur in the keycodes used to represent some of the functions.

A program loaded into the HP-67 or HP-97 is not permanent-once the calculator is turned off, the program will not be retained. You can, however, permanently save any program by recording it on a blank magnetic card, several of which were provided in the Standard Pac that was shipped with your calculator. Consult your Owner's Handbook for full instructions. A few points to remember:

The Set Status section indicates the status of flags, angular mode, and display setting. After keying in your program, review the status section and set the conditions as indicated before using or permanently recording the program.
REMEMBER! To save the program permanently, clip the corners of the magnetic card once you have recorded the program. This simple step will protect the magnetic card and keep the program from being inadvertently erased.

As a part of HP's continuing effort to provide value to our customers, we hope you will enjoy our newest concept.

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CARDIAC PROGRAM SERIES

The following programs may be used in a series to carry out the many calculations in a particular medical procedure. Following are examples from an adult cath lab and a pediatric cath lab. These examples are fairly complicated. Before attempting them, read over the detailed instructions for each of the programs and try the included examples. In these examples, values stored in memory for later use are underlined. When recalled from memory (so that they do not need to be reentered), they are enclosed in brackets.

## Adult Cath Lab Example:

Note that cardiac output, calculated in DYE CURVE CARDIAC OUTPUT is used in BODY SURFACE AREA and VALVE AREA and STROKE WORK. BODY SURFACE AREA, calculated by the Du Bois method, is used in STROKE WORK.

## Program

| DYE CURVE <br> CARDIAC OUTPUT | $\begin{aligned} & \Delta \mathrm{t}=1 \mathrm{sec} . ; \\ & \mathrm{DC}=38,67,80,73,61, \\ & 48,36,29 \mathrm{Div} ; \\ & \mathrm{CAL}=0.11 \mathrm{mg} / 1 / \mathrm{Div} ; \\ & \text { DOSE }=5.6 \mathrm{mg} \end{aligned}$ | $\begin{aligned} & \text { AREA }=532.60 \mathrm{Div} \mathrm{sec} ; \\ & \mathrm{CAL} \times \mathrm{AREA}=58.59 \mathrm{mg} / 1 \\ & \mathrm{CO}=5.731 / \mathrm{min} \end{aligned}$ |
| :---: | :---: | :---: |
| BODY SURFACE <br> AREA (Du Bois) | Ht. = -72.1 in., Wt.= -191 lb. (CO) | $\begin{aligned} & \mathrm{Ht} .=183.13 \mathrm{~cm} ; \\ & \mathrm{Wt}=86.82 \mathrm{~kg} . \\ & \mathrm{BSA}=2.09 \mathrm{~m}^{2} \\ & \mathrm{CI}=2.741 / \mathrm{min} / \mathrm{m}^{2} \end{aligned}$ |
| VALVE AREA (Aortic) | $\begin{aligned} & \mathrm{SEP}=0.2 \mathrm{sec} ; \\ & \Delta \mathrm{P}=38,45,40,31 \mathrm{mmHg} ; \\ & \mathrm{R}-\mathrm{R}=0.92 \mathrm{sec} . \\ &(\mathrm{C} 0) \end{aligned}$ | $\begin{aligned} \Delta \mathrm{P} & =38.50 \mathrm{mmHg} \\ \text { AREA } & =1.59 \mathrm{~cm}^{2} \end{aligned}$ |
| VALVE AREA (Mitral) | $\begin{aligned} \mathrm{DFP} & =0.55 \mathrm{sec} ; \\ \Delta \mathrm{P} & =10,12,8,6,2 \mathrm{mmHg} ; \\ \mathrm{R}-\mathrm{R} & =0.94 \mathrm{sec} ; \quad(\mathrm{CO}) \end{aligned}$ | $\begin{gathered} \Delta \mathrm{P}=7.60 \mathrm{mmHg} ; \\ \text { AREA }=-1.90 \mathrm{~cm}^{2} \end{gathered}$ |
| STROKE WORK | $\begin{aligned} & P_{\text {sys }}=155,169,165,152, \\ & 138 \mathrm{mmHg} ; \\ & R-R=0.92 \mathrm{sec} ; \quad(C 0) \quad(B S A) \end{aligned}$ | $\begin{aligned} & \Delta \mathrm{P}=155.80 \mathrm{mmHg} ; \\ & \mathrm{SW}=186.17 \mathrm{gm} \cdot \mathrm{~m} \\ & \mathrm{SWI}=88.95 \mathrm{gm} \cdot \mathrm{~m} / \mathrm{m}^{2} \end{aligned}$ |
| CONTRACTILITY | $\begin{aligned} \mathrm{t}= & 0.01 \mathrm{sec} ; \\ \mathrm{P}_{\mathrm{N}}= & 14.8,28.5,51.7, \\ & 81.8,105.6 \end{aligned}$ | $\begin{aligned} & \operatorname{MAX} \mathrm{dP} / \mathrm{dt}=3010 \mathrm{mmHg} / \mathrm{sec} \\ & \mathrm{MAX} \mathrm{dP} / \mathrm{dt} / \mathrm{P}=63.3 \mathrm{sec} ; \\ & \mathrm{V}_{\mathrm{MAX}}=2.49 \mathrm{circ} / \mathrm{sec} \end{aligned}$ |

## Pediatric Cath Lab Example:

Note that body surface area calculated in BODY SURFACE AREA (Boyd) is used in FICK Cardiac output. Venous oxygen content, calculated the first time $0_{2}$ SATURATION and CONTENT is run, is used in FICK. Hemoglobin, entered the first time SAT is run, automatically reappears the second time. Especially note that arterial oxygen content is left in the display the second time SAT is run, and is ready as the first entry in FICK. This is another method of transferring data between programs.

## Program

| BODY SURFACE AREA (Boyd) | Ht. $=55 \mathrm{~cm} ; \mathrm{Wt}=4.2 \mathrm{~kg}$ | $\underline{B S A}=0.26 \mathrm{~m}^{2}$ |
| :---: | :---: | :---: |
| $0_{2}$ SATURATION and CONTENT (Venous) | $\begin{aligned} & \mathrm{PO}_{2}=30 \mathrm{mmHg} \\ & \text { Sat. }=55 \% ; \mathrm{Hgb}=18 \mathrm{gm} / 100 \mathrm{ml} \end{aligned}$ | $\begin{aligned} & \text { Est. Sat. }=57.18 \% \\ & \mathrm{C}_{\mathrm{V}} 0_{2}=13.36 \mathrm{Vo} 1 . \% \end{aligned}$ |
| $0_{2}$ SATURATION and CONTENT (Arterial) | $\mathrm{PO}_{2}=52 \mathrm{mmHg} ;$ Sat. $=84.5 \%$ (Hgb) | $\begin{aligned} & \text { Est. Sat. }=86.86 \% \\ & \mathrm{CaO}_{2}=20.54 \mathrm{Vol} . \% \end{aligned}$ |
| FICK CARDIAC OUTPUT | $\begin{aligned} & \left(\mathrm{CaO}_{2}\right) ;\left(\mathrm{C}_{\mathrm{V}} \mathrm{O}_{2}\right) ; \\ & \mathrm{VO}_{2}=60 \mathrm{ml} / \mathrm{min} \\ & (\mathrm{BSA}) ; \mathrm{HR}=95 \mathrm{BPM} \end{aligned}$ | $\begin{aligned} \mathrm{CO} & =0.84 \mathrm{l} / \mathrm{min} \\ \mathrm{CI} & =3.15 \mathrm{l} / \mathrm{min} / \mathrm{m}^{2} \\ \mathrm{SV} & =8.74 \mathrm{~m} 1 \\ \mathrm{SI} & =-33.14 \mathrm{ml} / \mathrm{m}^{2} \end{aligned}$ |
| ANATOMIC SHUNTS | $\begin{aligned} & \text { R-SYST }=55 \% ; \text { R-PUL }=62 \% \\ & \text { L-SYST }=84.5 \% ; \text { L-PUL }=97 \% \end{aligned}$ | $\begin{array}{ll} \text { L-R } & \text { SHUNT }=16.67 \% \\ \text { R-L } & \text { SHUNT }=-29.76 \% \end{array}$ |

# Program Title YIRTUAL $\mathrm{PO}_{2}$ AND $\mathrm{O}_{2}$ SATURATION AND CONTENT 

Contributor's Name Hewlett-Packard Company
Address 1000 N.E. Circle Boulevard
City Corvallis State Oregon

Program Description, Equations, Variables The first part of this program computes virtual $\mathrm{PO}_{2}$ for use in estimating $\mathrm{O}_{2}$ saturation. Generally, it will be more convenient to calculate venous values first, as arterial values are frequently needed in other programs and, thus, will be left in the storage registers after both calculations.

The equation solved is

$$
\mathrm{VPO}_{2}=\mathrm{PO}_{2} \cdot 10^{\left[0.024(37-\mathrm{BT})+0.48(\mathrm{pH}-7.4)+0.06\left(1 \mathrm{ogPCO}_{2}\right)\right]}
$$

which is a hybrid of the equation used by Thomas and that used by Kelman. There is some disagreement regarding the best value of the pH multiplier, 0.48 being used by most workers, but see, for example, Kelman.

The second part of the program estimates $0_{2}$ saturation of blood from virtual $\mathrm{PO}_{2}$ and computes $\mathrm{O}_{2}$ content. If the actual $\mathrm{O}_{2}$ saturation is known, $\mathrm{O}_{2}$ content may be computed directly.

## Equations:

The part of the program for estimating $0_{2}$ saturation is based on the polynomial curve fit of Thomas, where $\mathrm{VPO}_{2}$ is in mmg.

$$
0_{2} \text { Sat }=\frac{\left(\mathrm{VPO}_{2}\right)^{4}-15\left(\mathrm{VPO}_{2}\right)^{3}+2045\left(\mathrm{VPO}_{2}\right)^{2}+2000\left(\mathrm{VPO}_{2}\right)}{\left(\mathrm{VPO}_{2}\right)^{4}-15\left(\mathrm{VPO}_{2}\right)^{3}+2400\left(\mathrm{VPO}_{2}\right)^{2}-31,100\left(\mathrm{VPO}_{2}\right)+2,400,000}
$$

This calculation assumes that the oxygen dissociation curve for the hemoglobin is normal. The $\mathrm{O}_{2}$ content is computed from

$$
\mathrm{C}_{\mathrm{x}} \mathrm{O}_{2}(\mathrm{Vol} . \%)=1.34 \cdot \frac{\mathrm{SAT}(\%)}{100} \cdot \mathrm{Hgb}(\mathrm{~g} / 100 \mathrm{ml})+0.0031 \mathrm{PO}_{2} \text { (mming) }
$$

Operating Limits and Warnings Virtual $\mathrm{PO}_{2}$ is not in any way a real physiologic $\mathrm{PO}_{2}$. Its only function is for use in estimating $O_{2}$ saturation, and it should never be confused with $\mathrm{PO}_{2}$ corrected to body temperature. Furthermore, it must always be calculated from blood parameters measured at or corrected to $37^{\circ} \mathrm{C}$. The calculation will give inaccurate results for fetal hemoglobin, present in babies less than six months old, and for some abnormal adult hemoglobins and certain other blood conditions. The results of the estimation and any subsequent calculations based on it, should be viewed with caution unless the dissociation curve has been previously established to be normal. If both $\mathrm{PO}_{2}$ and $\mathrm{O}_{2}$ saturation are measured, the program may be used as a convenient mean to check for the normality of the dissociation curve.

[^0]DETAILED USER INSTRUCTIONS:
Input $\mathrm{PO}_{2}, \mathrm{PCO}_{2}$, and pH measured at $37^{\circ} \mathrm{C}$. Input body temperature in degrees C. If $\mathrm{PO}_{2}$ has been previously input, recall it by pressing [f] [A] then press [f] [B]. Otherwise, input $\mathrm{PO}_{2}$ and press [f] [B]. For each variable after $\mathrm{PO}_{2}$, stored values will be recalled. If none have been input, recalled values will generally be zero. It is important to input pH and body temperature exactly, as these have a great influence on the calculation of virtual $\mathrm{PO}_{2}$. Errors, especially in body temperature, can result in large errors in $\mathrm{VPO}_{2}$ and, hence, estimated saturation. $\mathrm{PCO}_{2}$ has relatively little influence. Press the buttons from left to right and do not skip any. The virtual $\mathrm{PO}_{2}$ remains in the display for immediate entry in calculation of $\mathrm{O}_{2}$ saturation and content. It is not stored in place of the measured $\mathrm{PO}_{2}$. The $\mathrm{PO}_{2}, \mathrm{PCO}_{2}$, and pH remain in memory. Note that separate storage registers are not maintained for arterial and venous values, only the most recent ones will be stored.

To compute $0_{2}$ content, input the $\mathrm{PO}_{2}, \mathrm{O}_{2}$ saturation, and hemog1obin concentration. After $\mathrm{PO}_{2}$ is input, an estimated $\mathrm{O}_{2}$ saturation is calculated, based on a standard dissociation curve. This will only be meaningful if a virtual $\mathrm{PO}_{2}\left(\mathrm{VPO}_{2}\right)$ from the first part of the program is input. The estimated $\mathrm{O}_{2}$ saturation may be accepted simply by pressing [B], or a measured value can be input. If Hgb was previously input, it will be recalled. If the calculated $0_{2}$ content is to be stored as arterial or venous for later use in Fick cardiac output or physiologic shunt calculations, press the appropriate button. Regardless of which content is computed first, $\mathrm{CaO}_{2}$ is left in the display for convenience in case the ANATOMIC SHUNTS program is to be run next.

If $\mathrm{O}_{2}$ saturation of blood is to be estimated from $\mathrm{PO}_{2}$, it is important to input the virtual $\mathrm{PO}_{2}$ calculated in the first part of the program. A large error can result from inputting measured $\mathrm{PO}_{2}$ without the corrections. The program may be used to compare estimated $0_{2}$ saturation with measured $0_{2}$ saturation, to obtain a rough idea of the variation of the dissociation curve from normal. This will be especially sensitive with partly unsaturated venous blood where the slope of the curve is fairly steep. When computing content for purposes of estimating physiologic shunt and Fick cardiac output, it is always best to measure the saturation. Small variations in the dissociation curve can cause considerable error in the shunt and cardiac output calculations and because the effect is not the same on venous blood as on the higher saturation arterial blood.

The calculated $0_{2}$ content includes both the dissolved oxygen and the hemoglobin bound oxygen. If only $\mathrm{O}_{2}$ saturation was measured, and not $\mathrm{PO}_{2}$, an estimated $\mathrm{PO}_{2}$ should be input to obtain the maximum accuracy in the content calculation. The estimate for $\mathrm{PO}_{2}$ need only be rough as the effect is very small, unless the patient is breathing an oxygen-enriched atmosphere and $\mathrm{PO}_{2}$ is well above 100 mmHg .

To compute equivalent alveolar blood $O_{2}$ content, enter the equivalent $P_{A} 0_{2}$, rather than the virtual $\mathrm{PO}_{2}$. The $\mathrm{P}_{\mathrm{A}} \mathrm{O}_{2}$ can be calculated by the $\mathrm{A}-\mathrm{aO} \mathrm{O}_{2}$ DIFFERENCE program. In this case, the resulting $0_{2}$ content should not be stored as either arterial or venous, but simply left in the display register
for use at the beginning of the PHYSIOLOGIC SHUNT AND FICK programs which should be executed next. Thus, the over-all sequence should be to compute venous content first, arterial content second, and alveolar content last. The PHYSIOLOGIC SHUNT AND FICK program may then be run without having to enter any new $O_{2}$ content data.

## Progiram IDescription II



## Sample Problem(s)

1) For the following patient data calculate virtual $\mathrm{PO}_{2}$ and from it estimated $0_{2}$ saturation and $0_{2}$ content. Store the value as venous $0_{2}$ content.

$$
\begin{aligned}
\mathrm{PO}_{2} & =75 \mathrm{mmHg} \\
\mathrm{PCO}_{2} & =45 \mathrm{mmHg} \\
\mathrm{pH} & =7.35 \\
\mathrm{BT} & =40^{\circ} \mathrm{C} \\
\mathrm{Hgb} & =16 \mathrm{gm} / 100 \mathrm{ml}
\end{aligned}
$$

2) Calculate est. $\mathrm{O}_{2}$ saturation and $\mathrm{O}_{2}$ content assuming the $\mathrm{PO}_{2}$ was actually 75 mmHg .

Solution(s) 1) 75 [f] [B] 45 [f] [C] 7.35 [f] [D] 40 [f] [E] $\rightarrow 59.71 \mathrm{mmHg} \mathrm{VPO}_{2}$
[A] $\rightarrow 90.92$ est. SAT\%
[B] $16[C] \rightarrow 19.680_{2}$ Content \%
$[\mathrm{E}] \rightarrow 0.00$
( $19.68 \%$ stored as venous $0_{2}$ content. No previously stored arterial $\mathrm{O}_{2}$ content is present.)
2) $[f][A][A] \rightarrow 95.08$ est SAT\%
[B] $[C] \rightarrow 20.620_{2}$ Content

Reference(s) Thomas, L.J. Jr., "Algorithms for Selected Blood Acid-Base and Blood Gas Calculations," J. Appl. Physiol. 33: 154-158, 1972

Kelman, G. Richard, "Digital Computer Subroutine for the Conversion of Oxygen Tension into Saturation," J. App1. Physio1. 21: 1375-1376, 1966. This program is a modification of the Users' Library Programs \# 00196A and 非 00197A submitted by Hewlett-Packard.





## Program Description

Program Title BODY SURFACE AREA FOR CARDIO PULMONARY

Contributor's Name Hewlett-Packard Company
Address 1000 N.E. Circle Boulevard
City Corvallis
State Oregon
Zip Code 97330

Program Description, Equations, Variables This program calculates body surface area by either the method of DuBois or the method of Boyd. In both cases, the required inputs are height and weight, which may be input either in metric ( $\mathrm{cm}, \mathrm{kg}$ ) or English (in., 1b.) units. Quantities in English units should be input as negative numbers. If cardiac output is given, the cardiac index can also be calculated.

Equations:
Let Ht be height, Wt be weight, and BSA be the body surface area in $\mathrm{m}^{2}$.
$\mathrm{Ht}(\mathrm{cm})=2.54 \mathrm{Ht}$ (in.)
$\mathrm{Wt}(\mathrm{kg})=0.45359237 \mathrm{Wt}$ (1b.)

Du Bois:

$$
\text { BSA }\left(\mathrm{m}^{2}\right)=\mathrm{Ht}(\mathrm{~cm})^{0.725} \cdot \mathrm{Wt}(\mathrm{~kg})^{0.425} \cdot 7.184 \times 10^{-3}
$$

Boyd:

$$
\begin{aligned}
\mathrm{BSA}\left(\mathrm{~m}^{2}\right) & =\mathrm{Wt}(\mathrm{~g})^{0.7285-0.0188 \log \mathrm{Wt})} \cdot \mathrm{Ht}(\mathrm{~cm})^{0.3} \cdot 3.207 \times 10^{-4} \\
\mathrm{CI} & =\frac{\mathrm{CO}(1 / \mathrm{min})}{\mathrm{BSA}\left(\mathrm{~m}^{2}\right)}
\end{aligned}
$$

Operating Limits and Warnings The Du Bois formula for BSA is undefined for children with a BSA less than $0.6 \mathrm{~m}^{2}$. In such cases BSA should be calculated by the Boyd formula.

[^1]

## Sketch(es)

Sample Problem(s) 1) Patient is 176 cm in height and weighs 63.5 kg . What is his body surface area by both the DuBois and Boyd methods?
2) A patient 60 inches in height and 100 pounds in weight has a cardiac output of $51 / \mathrm{min}$. Calculate the body surface area and cardiac index by DuBois. What is the cardiac index using the Boyd BSA?

Solution(s) 1) 176 [A] 63.5 [B] [C] $\rightarrow 1.78 \mathrm{~m}^{2}$ (DuBois)
$[\mathrm{D}] \rightarrow 1.76 \mathrm{~m}^{2}$ (Boyd)
2) 60 [CHS ] [A] 100 [CHS] [B] [C] $\rightarrow 1.39 \mathrm{~m}^{2}$ (DuBois)
$5[\mathrm{E}] \rightarrow 3.591 / \mathrm{min} \mathrm{m}^{2}$ (CI, DuBois)
[D] $\rightarrow 1.40 \mathrm{~m}^{2}$ (Boyd)
[f] [E] $\rightarrow 5.00$ (Recalls CO, Stored above)
$[\mathrm{E}] \rightarrow 3.571 / \mathrm{min} \mathrm{m}^{2}$ (CI, Boyd)

Reference(s) D. DuBois and E.F. DuBois, C1in. Cal. 10, Arch. Int. Med., 17, 863,1916. Edith Boyd, Growth of the Surface Area of the Human Body, U. of Minnesota Press, 1935, p. 132.
 \# 00204A submitted by Hewlett-Packard.

1 BODY SURFACE AREA for CARDIO PULMONARY
RCL CO
Height
Weight
DuBois
Boyd
$\mathrm{CO} \rightarrow \mathrm{CI}$


| STEP K | KEY ENTRY | KEY CODE | COMments | StEP |  | Key entry | key code | COMMENTS |
| :---: | :---: | :---: | :---: | :---: | :---: | :---: | :---: | :---: |
| Qe: | *-ELS | 2111 | Enter Ht. <br> If cm store |  | 5 |  | -62 |  |
| 60. | N0? | 16-44 |  |  | 58 | 3 | 83 |  |
| 06. | 0701 | 2201 |  |  | 59 | $Y^{*}$ | 31 |  |
| 064 | CHS | -22 | If inches, convert to cm and store |  | 60 | RCLE | 3606 |  |
| 005 | 2 | 62 |  |  | 61 | EEX | -23 |  |
| 806 | . | -62 |  |  | 62 | 3 | 83 |  |
| 007 | 5 | 45 |  |  | E | $x$ | -35 |  |
| 000 | 4 | 04 |  |  | 64 | ENT¢ | -21 |  |
| 009 | - $x$ | -35 |  |  | 65 | LOG | 1632 |  |
| 010 | NLELI | 2101 |  |  | 66 | . | -62 |  |
| 011 | 5105 | 3505 | Store Ht. |  | 67 | 9 | 00 |  |
| 012 | RTN | 24 | Store Ht. |  | 68 | 1 | 81 |  |
| 013 | *LELE | 2112 | Enter Wt. <br> If kg store |  | 69 | 8 | 88 |  |
| 014 | K0? | 16-44 |  |  | 70 | 8 | 88 |  |
| 815 | GT02 | 2208 |  |  | 71 | $x$ | -35 |  |
| 816 | CHE | -22 | If lbs., convert to kg and store |  | 72 | . | -62 |  |
| 017 | 2 | 02 |  |  | 3 | 7 | 07 |  |
| 018 |  | -62 |  |  | 74 | 2 | 02 |  |
| 019 | 2 | 02 |  |  | 75 | 8 | 08 |  |
| 020 | $\div$ | -24 |  |  | 76 | 5 | 85 |  |
| 021 | *lele | 21.42 |  |  | 77 | - | -45 |  |
| 022 | Stue | 3506 | Store Wt. |  | 78 | $\psi^{x}$ | 31 |  |
| 023 | RTH | 24 |  |  | 79 |  | -24 |  |
| 024 | *LELC | 2113 | Calculate BSA by DuBois |  | 80 | 3 | 03 |  |
| 025 | RCL5 | 3605 |  |  | 81 | 1 | 01 |  |
| 026 | - | -62 |  |  | 82 | 1 | 01 |  |
| 927 | 7 | 87 |  |  | 83 | 8 | 08 |  |
| 028 | 2 | Q2 |  |  | 84 | $\div$ | -24 |  |
| 029 | 5 | 05 |  |  | 85 | stot | 3501 |  |
| 030 | - ${ }^{\text {\% }}$ | 31 |  |  | 86 | EEX | -23 | Tangle with CO and store as 100 CO + . 01 BSA |
| 031 | RCLE | 3606 |  |  | 87 | 2 | 02 |  |
| 032 |  | -62 |  |  | 88 | $\div$ | -24 |  |
|  | 4 | 64 |  |  | 89 | RCLT 7 | 3687 |  |
| 034 | 2 | 02 |  |  | 90 | INT | 1634 |  |
| 035 | 5 | 05 |  |  | 91 | + | -55 |  |
| 036 | $\gamma^{x}$ | 31 |  |  | 92 | stor | 3507 |  |
| 037 | - $x$ | -35 |  |  | 93 | RCLI | 3601 |  |
| 038 | 1 | 01 |  |  | 94 | PRTX | -14 |  |
| 039 | 3 | 03 |  |  | 95 | RTN | 24 |  |
| 046 | 9 | 09 |  |  | 96 | *LELe | 211615 | Untangle and |
| 641 | . | -62 |  |  | 97 | FCL 7 | 3607 | recall CO |
| 042 | 2 | 02 |  |  | 98 | EEX | -23 |  |
| 043 |  | -24 |  |  | 99 | 2 | 02 |  |
| 044 | ST01 | 3501 |  |  | $0 \cdot$ | $\div$ | -24 |  |
| 045 | EE\% | -23 | ```Tangle with CO and store as 100 CO + . . 01 BSA``` |  | 01 | RTN | 24 |  |
| 046 | 2 | 02 |  |  | 02 | *LBLE | 2115 | Calculate CI |
| 047 | $\stackrel{\square}{\square}$ | -24 |  |  | 03 | EEX | -23 | untangle CO with |
| 1148 | RCLT | 3607 |  |  | 04 | 2 | 02 | BSA and store |
| 049 | INT | 1634 |  |  | 85 | $x$ | -35 |  |
| 050 | $\xrightarrow[+]{+}$ | -55 |  |  | 96 | INT | 1634 |  |
| 851 | stor | 3587 |  |  | 18 | RCL 7 | 3607 |  |
| 052 | FCL1 | 3601 |  |  | 88 | FRC | 1644 |  |
| 053 | FRTX | -14 |  |  | 09 | $+$ | -55 |  |
| 054 | RTN | 24 |  |  | 10 | ST07 | 3507 |  |
| 055 | VIBLD | 2114 | Calculate BSA by Boyd |  | 11 | LSTX | 16-63 |  |
| REGISIEHS |  |  |  |  |  |  |  |  |
| 0 | B | ${ }^{2}$ | ${ }^{3} \quad{ }^{4}$ |  |  | ${ }^{6}$ | 7 | 9 |
|  | BSA |  |  | HT. |  | WT. | Used |  |
| so | S1 | S2 | S3 | S5 |  | S6 | 57 | S8 |
| A | B |  | c | D |  |  | E ${ }^{\text {E }}$ |  |




## Program Description, Equations, Variables, etc.

This program computes the area of the first part of the curve by trapezoidal rule integration. The part after the last point is calculated from an exponential projection based on the first measured point below $65 \%$ of the peak measured point; and the first measured point after that which is below $45 \%$ of the peak. This not only avoids problems of indicator recirculation in most cases, but also limits the amount of data to be input. Thus it is important to have a measured point which is below $45 \%$ of the peak, but before recirculation becomes obvious. If this isn't possible, an approximation can be obtained by guessing at the curve without recirculation and entering these values.
Equation Used:

$$
\mathrm{CO}(l / \mathrm{min})=\frac{\mathrm{DOSE}(\mathrm{mg}) \cdot 60(\mathrm{sec} / \mathrm{min})}{\mathrm{CAL}(\mathrm{mg} / l / \mathrm{div}) \cdot \operatorname{AREA}(\mathrm{div} \cdot \mathrm{sec})}
$$

## Operating Limits and Warnings

Although this program leaves CO stored in memory, it erases all other stored patient data, including BSA.

[^2]Detailed User Instructions
This program calculates cardiac output from measurements taken directly from an indicator dilution curve. To obtain accurate results, it is important to measure the curve at frequent intervals. Generally, about ten points on the curve, equally spaced in time between onset and the $40 \%$-of-peak point on the downslope, will be adequate. Choose a measurement time interval accordingly. Input the interval $(\Delta t)$ and press [A].

Input the values measured from the curve ( $D C$ ) and press [B] after each. The units of measurement are arbitrary; for example, divisions on the paper or volts, so long as the same units are used in inputting the calibration. The values are measured relative to the baseline, or starting level, of the curve. After each input entry, the display will indicate the number of points input.

As points on the downslope are input, the program compares each with the peak value. When the first point whose value is less than $65 \%$ of the peak value is found, it is stored for later use in the exponential projection as indicated by a minus sign preceding the displayed value representing the number of points input.

When a point having a value less than $45 \%$ of the peak value is input, the program automatically makes the exponential projection and displays the area under the curve, rather than the number of points entered.

At this time, input the CAL value. If indocyanine green dye is being used, it will generally be measured as milligrams of dye per liter of the patient's blood per division or unit of curve measurement. For other indicators, equivalent calibration factors must be determined.

Finally, input the dose of indicator given. For dye, this will usually be in mg. Press [D], and cardiac output in liters/min. will result. CO is stored in memory.

## Sketch(es)

## Sample Problem(s)

$\Delta \mathrm{t}=1 \mathrm{sec}$.
$\mathrm{DC}=5,2,45,60,50,38,28,20$ div.
$\mathrm{CAL}=0.2 \mathrm{mg} / \mathrm{l} / \mathrm{div}$.
DOSE $=3 \mathrm{mg}$

Solution(s)

```
1[A] 5[B] 20[B] 45[B] 60[B] 50[B] 38[B] 28[B] 20[B] ------> 318.32 div/sec (area)
.2[C] 3[D] ----------------------------------------------- 2.--- 1/min. (co)
```

Reference (s)
Yang, Sing San, et al, From Cardiac Catheterization Data to Hemodynamic Parameters,
F.A. Davis Co., Phil., 1972.

This program is a translation of the HP-65 Users' Library program \#00205A submitted by Hewlett-Packard.

## User Instructions




## Program Description



## Program Description, Equations, Variables, etc.

This program computes cardiac output, stroke volume, and cardiac index by the Fick method.

Equations Used:

$$
\begin{gathered}
\mathrm{CO}(l / \mathrm{min})=\frac{\mathrm{VO}_{2}(\mathrm{ml} / \mathrm{min} \mathrm{STPD}) \cdot 100(\%)}{\left(\mathrm{C}_{\mathrm{a}} \mathrm{O}_{2}-\mathrm{C}_{\mathrm{v}} \mathrm{O}_{2}\right)(\mathrm{vol} . \%) \cdot 1000(\mathrm{ml} / \mathrm{l})} \\
\mathrm{SV}(\mathrm{ml} / \mathrm{beat})=\frac{\mathrm{CO}(l / \mathrm{min}) \cdot 1000(\mathrm{ml} / \mathrm{l})}{\mathrm{HR}(\text { beats } / \mathrm{min})} \\
\mathrm{CI}\left(l / \mathrm{min} / \mathrm{m}^{2}\right)=\frac{\mathrm{CO}(l / \mathrm{min})}{\mathrm{BSA}\left(\mathrm{~m}^{2}\right)} \\
\mathrm{SI}\left(\mathrm{ml} / \mathrm{m}^{2}\right)=\frac{\mathrm{SV}(\mathrm{ml})}{\mathrm{BSA}\left(\mathrm{~m}^{2}\right)}
\end{gathered}
$$

Operating Limits and Warnings

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## Sketch(es)

$\square$

## Reference (s)

Yang, Sing San, et al, From Cardiac Catheterization Data to Hemodynamic Parameters,
F.A. Davis Co., Phil., 1972.

This program is a translation of the HP-65 Users' Library program \#00206A submitted by Hewlett-Packard.



## Program Description

Program Title
VALVE AREA

Contributor's Name Hewlet.t.-Packard
Address $\quad 1000$ N.E. Circle BTvd.
City
Corvallis
State Oreaon
Zip Code
$9733 n$

Program Description, Equations, Variables, etc.
This program calculates aortic valve area and mitral valve area.

Equations Used:

$$
\text { Valve Area }\left(\mathrm{cm}^{2}\right)=\frac{\text { Mean Flow }}{0.0445 \sqrt{\text { mean gradient }}}
$$

where

$$
\begin{gathered}
\text { Mean Flow }(l / \mathrm{sec})=\frac{\mathrm{CO}(l / \mathrm{min} .) \cdot \mathrm{R}-\mathrm{R}(\mathrm{sec})}{\text { Valve Open Time }(\mathrm{sec} / \mathrm{beat}) \cdot 60(\mathrm{sec} / \mathrm{min} .)} \\
\text { Mitral Valve Area only }=\frac{\text { Valve Area }}{0.7}
\end{gathered}
$$

Operating Limits and Warnings

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## Sketch(es)

Sample Problem(s)
$\mathrm{DFP}($ mitral valve $)=0.55 \mathrm{sec}$
$\Delta \mathrm{P}=10,12,8,6,2 \mathrm{mmHg}$
$R-R=0.94 \mathrm{sec}$
$\mathrm{CO}=5.73 l / \mathrm{min}$.

Solution(s)
[f] [A] --------> 1.00 (for mitral valve)
.55[A] 10[B] 12[B] 8[B] 6[B] 2[B] -----------> 5.0
[C] ----------> $7.60 \mathrm{mmHg}, \overline{\Delta \mathrm{P}}$
.94[D] $5.73[E]$-----------------------------> $1.90 \mathrm{~cm}^{2}$, AREA

Reference(s) Gorlin, R.; Gorlin, S.G., "Hydraulic Formula for Calculation of the Area of the Stenotic Mitral Valve, Other Cardiac Valves, and Central Circulatory Shunts", American Heart Journal, Jan. 1957, VOL. 41, No. 1.
This program is a modification of the Users' Library program \#00207A submitted by Hewlett-Packard.




Program Description, Equations, Variables, etc.
This program calculates left-to-right and right-to-left shunts and displays them as a percentage. The program uses the method of allegations and can calculate bi-directional shunts.

Equations Used:

$$
\begin{aligned}
& \mathrm{R}-\mathrm{L} \operatorname{shunt}(\%)=\frac{(\mathrm{L}-\mathrm{PUL})-(\mathrm{L}-\mathrm{SYST})}{(\mathrm{L}-\mathrm{PUL})-(\mathrm{R}-\mathrm{SYST})} \cdot 100 \\
& \mathrm{~L}-\mathrm{R} \operatorname{shunt}(\%)=\frac{(\mathrm{R}-\mathrm{PUL})-(\mathrm{R}-\mathrm{SYST})}{(\mathrm{L}-\mathrm{PUL})-(\mathrm{R}-\mathrm{SYST})} \cdot 100
\end{aligned}
$$

Operating Limits and Warnings

This program has been verified only with respect to the numerical example given in Program Description II. User accepts and uses this program material AT HIS OWN RISK, in reliance solely upon his own inspection of the program material and without reliance upon any representation or description concerning the program material.
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## Sketch(es)

## Sample Problem(s)

Calculate the left-to-right or right-to-left shunts for a patient having the following oxygen saturation values at the listed sites. Right atrium, $85 \%$; pulmonary artery, $88 \%$; left atrium, $95 \%$; left ventricle, 93\%.

## Solution(s)

85[A] 88[B] $95[\mathrm{C}] 93[\mathrm{D}]$ [E] $-\cdots-\cdots 30.00 \%$ (L-R Shunt)
[E] --------> -20.00\% (R-L) Shunt)

## Reference (s)

Zimmerman, H.A., Intravascular Catheterization, Charles C. Thomas, Springfield, Ill., 1966.

This program is a translation of the HP-65 Users' Library program \#00208A submitted by Hewlett-Packard



## Program Description

Program Title

| Contributor's | Name $\quad$ Hewlett-Packard |  |  |  |  |
| :--- | :--- | :--- | :--- | :--- | :--- | :--- |
| Address | 1000 N.E. Circle Blvd. |  |  |  |  |
| City | Corvallis | State | Oregon | Zip Code | 97330 |

## Program Description, Equations, Variables, etc.

This program calculates the indices of left ventricular contractility based on pressure rise during isovolumetric contraction.

Equations Used:

| $\mathrm{P}_{\mathrm{N}}$ | $=$ most recently entered pressure (mmHg) |
| :--- | :--- |
| $\mathrm{P}_{\mathrm{N}-1}$ | $=$ next previously entered pressure |
| $\Delta t$ | $=$ time interval between pressure measurements (sec) |
| $\mathrm{P}_{\mathrm{P}}$ | $=$ pressure at which dP/dt/P is calculated |
| $\Delta \mathrm{P}$ | $=\mathrm{P}_{\mathrm{N}}-\mathrm{P}_{\mathrm{N}-1}$ |
| $\frac{d \mathrm{P}}{\mathrm{dt}}$ | $=\frac{\Delta \mathrm{P}}{\Delta t} \mathrm{mmHg} / \mathrm{sec}$ |
| $\mathrm{P}_{\mathrm{P}}$ | $=\frac{\mathrm{P}_{\mathrm{N}}+\mathrm{P}_{\mathrm{N}-1}}{2}$ |
| $\mathrm{dP} / \mathrm{dt} / \mathrm{P}$ | $=\frac{\mathrm{dP} / \mathrm{dt}}{\mathrm{P}_{\mathrm{P}}} \sec ^{-1}$ |
| $\mathrm{P}_{\mathrm{M}}$ | $=\mathrm{P}_{\mathrm{P}}$ where dP/dt/P is a maximum |
| $V_{\mathrm{MAX}}$ | $=\frac{1}{30} \frac{\left(\mathrm{P}_{\mathrm{PLAST}} \cdot \mathrm{MAX} \mathrm{dP} / \mathrm{dt} / \mathrm{P}\right)-\left(\mathrm{P}_{\mathrm{M}} \cdot \mathrm{dP} / \mathrm{dt} / \mathrm{P}_{\mathrm{LAST}}\right)}{\mathrm{P}_{\mathrm{P}}}$ |

## Operating Limits and Warnings

This program has been verified only with respect to the numerical example given in Program Description II. User accepts and uses this program material AT HIS OWN RISK, in reliance solely upon his own inspection of the program material and without reliance upon any representation or description concerning the program material.

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| Program Title Contractility |  |  |  |  |
| :---: | :---: | :---: | :---: | :---: |
| Contributor's Name Hewlett-Packard |  |  |  |  |
| Address 1000 N.E. Circle Blvd. |  |  |  |  |
| City Corvallis | State | Oregon | Zip Code | 97330 |

Program Description, Equations, Variables, etc.
$\mathrm{dP} / \mathrm{dt}$ is calculated as the difference between successive pressure inputs divided by the time interval $\Delta \mathrm{t}$. The largest value found is stored as maximum $\mathrm{dP} / \mathrm{dt}$. $\mathrm{dP} / \mathrm{dt} / \mathrm{P}$ is calculated for each pair of successive inputs, by first determining $\mathrm{dP} / \mathrm{dt}$ as above, then dividing by the mean of the two pressures. The largest value found is stored as maximum $\mathrm{dP} / \mathrm{dt} / \mathrm{P}$.
$V_{\text {max }}$ is found in this program by a linear projection of the downslope of the $\mathrm{dP} / \mathrm{dt} / \mathrm{P}$ vs. P curve back to $\mathrm{P}=0$, and by dividing the resulting $\mathrm{dP} / \mathrm{dt} / \mathrm{P}$ by 30 . The projection is based on the point at which the maximum $\mathrm{dP} / \mathrm{dt} / \mathrm{P}$ was found, and the last point input. The constant is controversial, values between about 28 and 32 having appeared in the literature. The value 30 is used in this program.

Operating Limits and Warnings

[^3]
## Program Deseription II

## Sketch(es)

## Sample Problem(s)

Find maximum $\mathrm{dP} / \mathrm{dt}$, maximum $\mathrm{dP} / \mathrm{dt} / \mathrm{P}$ and maximum ventricular contractility if $\Delta \mathrm{t}$ is 0.005 seconds and $P_{N}$ is $10,20,40,60$, and 80 mmHg .

Solution(s)
. 005 [A] $10[B] 20[B] 40[B] 60[B] 80[B][C]---------\rightarrow 4000 \mathrm{mmHg} / \mathrm{sec}(\mathrm{dP} / \mathrm{dt})$
[D] ------------ $133.3 \mathrm{sec}^{-1}(\mathrm{MAX} . \mathrm{dP} / \mathrm{dt} / \mathrm{P})$
[E] ------------ $5.14 \mathrm{circ} / \mathrm{sec}\left(V_{\text {MAX }}\right)$

Reference(s)
Yang, Sing San, et al, "From Cardiac Catheterization Data to Hemodynamic Parameters",
F.A. Davis Co., Phil., 1972.

This program is a translation of the HP-65 Users' Library program \#00209A submitted by Hewlett-Packard.

| STEP | InStructions | INPUT DATA/UNITS |  | KEYS | OUTPUT DATA/UNITS |
| :---: | :---: | :---: | :---: | :---: | :---: |
| 1 | Enter program |  |  |  |  |
| 2 | Input $\Delta t$ | $\Delta \mathrm{t}$ (seconds) | A |  | $\Delta t$ (seconds) |
| 3 | Repeat step 3 for each $\mathrm{P}_{\mathrm{n}}$ | $\mathrm{P}_{1} \ldots \mathrm{P}_{\mathrm{n}}$ | B |  | $\mathrm{dP} / \mathrm{dt} / \mathrm{P}\left(\mathrm{sec}^{-1}\right)$ |
| 4 | Calculate maximum dP/dt |  | c |  | dP/dt(mmHg/ |
|  |  |  |  |  | $\mathrm{sec})$ |
| 5 | Calculate maximum dP/dt/P |  | D |  | $\mathrm{dP} / \mathrm{dt} / \mathrm{P}\left(\mathrm{sec}^{-1}\right)$ |
| 6 | Calculate $\mathrm{V}_{\text {max }}$ |  | E |  | $\mathrm{V}_{\text {max }}($ circ $/ \mathrm{sec}$ ) |
|  |  |  |  |  |  |
|  | DETAILED USER INSTRUCTIONS |  |  |  |  |
|  | The indices of left ventricular contractility | y calculate |  |  |  |
|  | by this program are based on the pressure rise | during |  |  |  |
|  | isovolumetric contraction. Measurements, equally | ly spaced |  |  |  |
|  | in time, should be input for the isovolumetric | phase only |  |  |  |
|  | Inputting values from the systolic ejection peri | iod can |  |  |  |
|  | cause significant errors. Generally, between 5 | and 10 |  |  |  |
|  | pressure measurements should be input, and the t | time inter |  |  |  |
|  | between measurements, $\Delta t$, chosen accordingly. T | Too few |  |  |  |
|  | measurements will cause the maximum values to be | e missed. |  |  |  |
|  | Too many will introduce excessive "noise" result | ting in |  |  |  |
|  | errors. |  |  |  |  |
|  | Input $t$ in seconds, for example, .005. Press | $s$ [ A ]. |  |  |  |
|  | Input left ventricular pressure measurements in | mmHg ; |  |  |  |
|  | press [B] after each. After each input except the | the first, |  |  |  |
|  | $\mathrm{dP} / \mathrm{dt} / \mathrm{P}$ for the two most recent points will be | displayed. |  |  |  |
|  | When all points have been input, press [C], [D] | and [E] |  |  |  |
|  | in any order to obtain the corresponding results | s-maximum |  |  |  |
|  | $\mathrm{dP} / \mathrm{dt}$, maximum $\mathrm{dP} / \mathrm{dt} / \mathrm{P}$ and $\mathrm{V}_{\text {MAX }}$, maximum velocilt | ty of the |  |  |  |
|  | contractile element at zero pressure in circumfer | erences or |  |  |  |
|  | lengths/sec. |  |  |  |  |
|  | If the contractility parameters are to be cal | 1culated |  |  |  |
|  | using developed pressure, or any pressure refere | ence other |  |  |  |
|  | than zero, perform the subtraction before enteri | ing |  |  |  |
|  | pressure values. |  |  |  |  |
|  |  |  |  |  |  |
|  |  |  |  |  |  |



| Program Title STROKE WORK |  |  |  |
| :---: | :---: | :---: | :---: |
| Contributor's Name Hewlett-Packard |  |  |  |
| Address 1000 N.E. Circle Blvd. |  |  |  |
| City Corvallis | State Oregon | Zip Code | 97330 |

## Program Description, Equations, Variables, etc.

This program calculates stroke work (SW) and stroke work index (SWI). For stroke work based on systolic minus end-diastolic pressure, perform subtraction before data input.

Equations Used:

$$
\begin{aligned}
& \mathrm{SW}(\mathrm{gm} \cdot \mathrm{~m})=\frac{13.6 \cdot \mathrm{P}(\mathrm{mmHg}) \cdot \mathrm{CO}(\mathrm{l} / \mathrm{min}) \cdot \mathrm{R}-\mathrm{R}(\mathrm{sec})}{60(\mathrm{sec} / \mathrm{min})} \\
& \mathrm{SWI}\left(\mathrm{gm} \cdot \mathrm{~m} / \mathrm{m}^{2}\right)=\frac{\mathrm{SW}(\mathrm{gm} \cdot \mathrm{~m})}{\mathrm{BSA}\left(\mathrm{~m}^{2}\right)}
\end{aligned}
$$

Operating Limits and Warnings

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## Sketch(es)

## Sample Problem(s)

$P_{\text {sys }}=100,110 \mathrm{mmHg}$
$\mathrm{R}-\mathrm{R}=1 \mathrm{sec}$
$\mathrm{CO}=5 \mathrm{l} / \mathrm{min}$.
$\mathrm{BSA}=2 \mathrm{~m}^{2}$

Solution(s)
100[A] $110[A][B]-2-105 \mathrm{mmHg}(\bar{P})$
1[C] 5[D] ------------------> $119.0 \mathrm{gm} \cdot \mathrm{m}(\mathrm{SW})$
2[E] ----n---------------> $59.50 \mathrm{gm} \cdot \mathrm{m} / \mathrm{m}^{2}($ SWI $)$

## Reference (s)

Yang, Sing San, et al, "From Cardiac Catheterization Data to Hemodynamic Parameters",
F.A. Davis Co., Phil., 1972.

This program is a translation of the HP-65 Users' Library program \#00210A submitted by Hewlett-Packard.


## 97 Program Listing I

| $4_{\text {STEP }}$ |  | KEY ENTRY | KEY Code | COMmENTS | STEP | $\mathrm{KE}$ | KEY ENTRY | key code | comments |  |
| :---: | :---: | :---: | :---: | :---: | :---: | :---: | :---: | :---: | :---: | :---: |
|  | 001 | *LELA | 2111 | Enter $P_{\text {sys }}$ <br> If first entry then INT else integrate Initialize |  | 057 | 5 TOG | 3509 |  |  |
|  | 602 | F1\% | 162301 |  |  | 058 | FRTX | $162^{-14}$ |  |  |
|  | 063 | $6 T 01$ | 2261 |  |  | 059 |  | 162201 |  |  |
|  | 004 | ST0: | 3501 |  |  | 060 | RTN | ${ }^{24}$ |  |  |
|  | 005 | , | 01 |  |  | 061 | RCL 7 | 3607 | Untangle | BSA |
|  | 006 | CHS | -22 |  |  | 062 | FRC | 1644 |  |  |
|  | 007 | STOI | 3546 |  |  | at3 | EEX | -23 |  |  |
|  | 069 | SFi | 162101 |  |  | 064 | 2 | 08 |  |  |
|  | 009 | 1 | 01 |  |  | 065 | x | -35 |  |  |
|  | 010 | FIN | 24 |  |  | 866 | R/S | 51 |  |  |
|  | 011 | *LELI | 2101 |  |  | 067 | *LELE | 2115 | Enter BSA |  |
|  | 012 | ST+1 | 35-55 61 |  |  | 068 | STO1 | 3541 |  |  |
|  | 013 | DSEI | 162546 |  |  | 069 | EEX | -23 | Tangle | with CO |
|  | 014 | FCLI | 3646 |  |  | 876 | 2 | 02 | Tangle | with 0 |
|  | 015 | CHE | -22 | Display count, $N$ |  | 071 | $\div$ | -24 |  |  |
|  | 016 | FTN | 24 | Compute $\overline{\mathrm{P}}$ |  | 072 | RCLT | 3687 |  |  |
|  | 017 | *LELE | 2112 | Compute P |  | 073 | INT | 1634 |  |  |
|  | 018 | RCL1 | 3601 |  |  | 974 | + | -55 |  |  |
|  | 019 | RCLI | 3646 |  |  | 975 | Stor | 3507 | Compute | WI |
|  | 020 | CHS | -22 |  |  | 076 | RCL9 | 3605 |  |  |
|  | 021 | $\because$ | -24 |  |  | 077 | RCLI | 3601 |  |  |
|  | 022 | $5 T 01$ | 3501 |  |  | 678 | $\div$ | -24 |  |  |
|  | 023 | PRTX | -14 |  |  | 679 | PRTX | -14 |  |  |
|  | 024 | CF1 | 162201 |  |  | 980 | RTN | 24 |  |  |
|  | 025 | RTN | 24 |  |  | $08:$ | Res | 51 |  |  |
|  | 026 | ALELC | 2113 | Enter R-R |  |  |  |  |  |  |
|  | 027 | ST08 | 3508 |  |  |  |  |  |  |  |
|  | 028 | RCLT | 3607 | Untangle CO |  |  |  |  |  |  |
|  | 029 | EEX | -23 |  |  |  |  |  |  |  |
|  | 030 | 2 | 02 |  |  |  |  |  |  |  |
|  | 031 | - | -24 |  |  |  |  |  |  |  |
|  | 032 | RTN | 24 |  |  |  |  |  |  |  |
|  | 033 | *LELD | 2114 | Enter CO |  |  |  |  |  |  |
|  | 034 | ENT $\uparrow$ | -21 |  | 090 |  |  |  |  |  |
|  | 035 | ENTT | -21 |  |  |  |  |  |  |  |
|  | 036 | EEX | -23 |  |  |  |  |  |  |  |
|  | 037 | 2 | 02 |  |  |  |  |  |  |  |
|  | -038 | $x$ | -35 |  |  |  |  |  |  |  |
|  | 039 | FRC | 1644 |  |  |  |  |  |  |  |
|  | 040 | RCLT | 3607 | Tangle CO with BSA |  |  |  |  |  |  |
|  | 041 | FRC | 1644 |  |  |  |  |  |  |  |
|  | 042 | + | -55 |  |  |  |  |  |  |  |
|  | 043 | Stor | 3507 |  |  |  |  |  |  |  |
|  | 044 | $R \downarrow$ | -31 | Compute stroke work | 100 |  |  |  |  |  |
|  | 845 | fCLE | 3608 |  |  |  |  |  |  |  |
|  | 046 | $\times$ | -35 |  |  |  |  |  |  |  |
|  | 047 | $\epsilon$ | 66 |  |  |  |  |  |  |  |
|  | 048 | 0 | $00^{0}$ |  |  |  |  |  |  |  |
|  | 049 | $\cdots$ | -24 |  |  |  |  |  |  |  |
|  | 050 | RCLI | 3601 |  |  | , | 0 FLAGS |  | SET STATUS |  |
|  | 051 | x | -35 |  |  |  |  | flags | trig | DISP |
|  | 052 | 3 | 01 |  |  |  | ¹P AVER. | $\bigcirc$ |  |  |
|  | 053 | 3 | 83 |  |  |  | $\frac{1}{}{ }^{\text {P }}$ AVER. | 0  <br> 1  <br> 1 $\square$ |  |  |
|  | 054 | - | -62 |  | 110 |  |  | 1  <br> 2  <br> 2 $\square$ | GRAD ${ }_{\text {RAD }}$ | SCl ENG $\square$ |
|  | 055 | ${ }^{6}$ | ${ }^{66}$ |  |  | 3 |  |  |  | ${ }_{\text {n }}$ |
|  | 056 | x | -35 | REGIS | Sters |  |  |  |  |  |
| 0 |  | ${ }^{1} \mathrm{P}, \overline{\mathrm{P}}, \mathrm{B}$ |  | ${ }^{3} \quad{ }^{4}$ | 5 |  | ${ }^{6}$ | ${ }^{7}$ Used | ${ }^{8}$ R-R | SW |
| so |  | S1 | S2 | S3 | 55 |  | S6 | 57 | S8 | S9 |
|  |  |  | B | Tc |  |  |  |  |  |  |
| A |  |  |  | c |  |  |  |  |  |  |

## Progiram Description

| Program Title Ejection Fraction - Ejected Volume - Cardiac Output |  |  |  |  |
| :---: | :---: | :---: | :---: | :---: |
| Contributor's Name Hewlett-Packard |  |  |  |  |
| Address $\quad 1000$ N.E. Circle Blvd. |  |  |  |  |
| City Corvallis | State | Oregon | Zip Code | 97330 |

Program Description, Equations, Variables
Given the following information: LED, LES, AED, AES, f and Heart Rate (HR).
$\underset{\text { (in percent) }}{\text { Ejection Fraction }}=\left[1-\frac{\text { AES }^{2}}{\text { AED }} \times \frac{\text { LED }}{\text { LES }}\right] \times 100$
$\underset{\text { (in cc/stroke) }}{\text { Ejected Volume }}=($ Ejection Fraction $) \times\left(\frac{8 \text { AED }^{2}}{3 \pi f^{3} L E D}\right) \div 100$ (in cc/stroke)

Cardiac Output = (Ejected Volume) x (Heart Rate) $\div 1000$ (in 1/min.)

Operating Limits and Warnings
Calulate ejection fraction before ejected volume, and ejected volume before cardiac output.

This program has been verified only with respect to the numerical example given in Program Description II. User accepts and uses this program material AT HIS OWN RISK, in reliance solely upon his own inspection of the program material and without reliance upon any representation or description concerning the program material.
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## Program Description II



Sample Problem(s)
Find the Ejection Fraction, Ejected Volume, and Cardiac Output from the following data.
$L E D=12.6 \mathrm{~cm}$
LES $=9.7 \mathrm{~cm}$
AED $=68.5 \mathrm{~cm}^{2}$
$A E S=23.2 \mathrm{~cm}^{2}$
$f=1.54: 1$
Heart Rate $=72 \mathrm{bpm}$

## Solution(s)

12.6 [ENT $\uparrow$ ] 9.7[A] 68.5[ENT $\uparrow$ ] 23.2[B]
1.54[ENT ] 72[f] [A] [C] ------------->85.10\% (Ejection Fraction)
[D] ------------->73.65\% (Ejected Volume)
[E] -------------> $5.30 \mathrm{l} / \mathrm{min}$. (CO)

Reference (s)
Doge, HT. Sandler, H. Ballew et al. "The use of biplane angio-cardiography for the measurement of left ventricular volume in man." American Heart J.60: 762-776 1960 Greene, D.G. Carlisle, R. Grant, C. Circulation 35: 61-69 1967. This program is a modification of the HP-65 Users' Library program \#01190A submitted by Norman R. McLarin.

EJECTION FRACTION - EJECTED
VOLUME-CARDIAC OUTPUT
f $\uparrow$ Rate
LED $\uparrow$ LES
AED $\uparrow$ AES
E F
E V
C 0

| STEP | instructions | $\begin{gathered} \text { INPUT } \\ \text { DATA/UNITS } \\ \hline \end{gathered}$ | KEYS |  | $\begin{gathered} \text { OUTPUT } \\ \text { DATA/UNITS } \\ \hline \end{gathered}$ |
| :---: | :---: | :---: | :---: | :---: | :---: |
| 1. | Load side 1 |  |  |  |  |
|  |  |  |  |  |  |
| 2. | Enter length end diastole and | LED, cm | ENT 1 |  |  |
|  | length end systole | LES, cm | A |  | LED, cm |
|  |  |  |  |  |  |
| 3. | Enter area end diastole and | AED, $\mathrm{cm}^{2}$ | ENT $\uparrow$ |  |  |
|  | area end systole | AES, $\mathrm{cm}^{2}$ | B |  | AED, $\mathrm{cm}^{2}$ |
|  |  |  |  |  |  |
| 4. | Enter correction factor $f$ and | $f$ | ENT $\uparrow$ |  |  |
|  | heart rate | HR, BPM | $f$ | A | $f$ |
|  |  |  |  |  |  |
| 5. | Calculate ejection fraction |  | C |  | E.F,\% |
|  |  |  |  |  |  |
| 6. | Calculate ejected volume |  | D |  | E.V., cc/s |
|  |  |  |  |  |  |
| 7. | Calculate cardiac output |  | E |  | C.0., 1/mi |
|  |  |  |  |  |  |
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| Calculation of Left Ventricular Functions from Angiograpic Data |  |  |  |  |
| :---: | :---: | :---: | :---: | :---: |
| Hewlett-Packard |  |  |  |  |
| Address 1000 N.E. Circle Blvd. |  |  |  |  |
| City Corvallis | State | Oregon | Zip Code | 97330 |

## Program Description, Equations, Variables

Program allows calculation of left ventricular functions by both single and biplane methods: Functions calculated are:
End systolic colume (ESV), either single or biplane
End diastolic volume (EDV), either single or biplane
Velocity of circumf. fiber shortening ( $V_{c f}$ )
Stroke volume
(SV)
Stroke index
Systolic ejection fraction as \% (SEF \%)
Heart Rate
Cardiac index (CI)

Equations:

$$
\begin{aligned}
& \text { Average systolic \& diastolic diameters are also calculated } \\
& \text { Equations: } \\
& \quad \text { Biplane } C V=\frac{8}{3 \pi} \quad \frac{\left(A_{R A O}\right)\left(\mathrm{CF}_{\mathrm{RAO}}\right)\left(\mathrm{A}_{\mathrm{LAO}}\right)}{\mathrm{L}_{\mathrm{RAO}}} \\
& \\
& \\
& \text { Single plane } \mathrm{CV}=\frac{8}{3 \pi} \frac{\left(\mathrm{~A}_{\mathrm{RAO}}\right)^{2} \times\left(\mathrm{CF}_{\mathrm{RAO}}\right)^{3 / 2}}{\mathrm{~L}_{\mathrm{RAO}}}
\end{aligned}
$$

True ventricular volumes: Biplane TV $=0.895 C V-5.113 \mathrm{ml}$ (where $\mathrm{CV}=$ Calc. volume) Single $\mathrm{TV}=0.81 C V+1.9 \mathrm{ml}$
SEE: Vogel, Swenson \& Elings,"Simple Method for Calculating Left Ventricular Function Etc.,"Catheterization \& Cardiovascular Diagnosis, 2:199-210 (1976) for complete description of calculations.
OPERATING LIMITS AND WARNINGS When using this program on HP-67 be sure pause display of results has finished blinking before pressing key for next calculation. Otherwise erroneous results may occur.

[^4]
## Program Description II

## Sketch(es)

Sample Problem(s) A patient's body surface area is $1.75 \mathrm{~m}^{2}$. Angiographic measurements give the following data:Number of frames: 19; number of frames per beat: 43; correction factors: 1.39(RAO), 0.83 (LAO)

Systolic Function

| RAO | LAO |
| ---: | ---: |
| 35.4 | 32.4 |
| 9.1 | 7.7 |


|  | Diastolic Function |  |
| :--- | :--- | :--- |
| RAO | LAO |  |
|  |  |  |
| AREA | 52.1 | 54.7 |
| AXIS | 10.5 | 10.0 |

Calculate left ventricular functions by both the single plane \& biplane methods.


Reference(s) This program is a modification of the HP-65 Users' Library program \#05352A submitted by J.H.K. Vogel.
Vogel, Swenson \& Elings, "A Simple Method for Calculating Left Ventricular Functions from Angiographic Data, Etc", Cathetherization and Cardio Vascular Diagnosis, 2: 199-210, (1976).


| STEP | instructions | $\begin{gathered} \text { INPUT } \\ \text { DATA/UNITS } \end{gathered}$ | KEYS |  | OUTPUT DATA/UNITS |
| :---: | :---: | :---: | :---: | :---: | :---: |
| 1. | Load sides 1 \& 2 |  |  |  |  |
| 2. | Enter data: Body surface area | BSA, ${ }^{2}$ | ENTT |  |  |
|  | Number of frames | \# | ENTA |  |  |
|  | Systolic area, RAO | SA, cm² | ENTA |  |  |
|  | Systolic length, RAO | SL, cm |  | E |  |
|  | Correction factor, RAO | CFRAO | ENTA |  |  |
|  | Number of frames/beat | \# | IENTH |  |  |
|  | Diastolic area, RAO | DA, $\mathrm{cm}^{2}$ |  |  |  |
|  | Diastolic Length, RAO | DL, cm | R/S |  |  |
|  | SINGLE PLANE CALCULATIONS: |  |  |  |  |
| 3. | Calculate: End systolic VOLO.(ESV) |  | A |  | ESV,m1 |
|  | and ESV index |  |  |  | $\mathrm{ESV} / \mathrm{m}^{2}$ |
|  |  |  |  |  |  |
| 4. | Calculate: End diastolic Vol., (EDV) |  | B |  | EDV,m1 |
|  | and EDV |  |  |  | $\mathrm{EDV} / \mathrm{m}^{2}$ |
|  |  |  |  |  |  |
| 5. | Calculate: Velocity of circumferential fiber |  |  |  |  |
|  | shortening, $V_{C f}$ |  | C |  | $\mathrm{V}_{\mathrm{cf}}, \frac{\mathrm{circ}}{\mathrm{sec}}$ |
|  |  |  |  |  |  |
| 6. | Calculate: Stroke volume and |  | D |  | SV, ml |
|  | stroke index |  |  |  | SI, ml/m² |
|  |  |  |  |  |  |
| 7. | Calculate: Systolic ejection fraction (\%) |  | E |  | SEF\% |
| 8. | Calculate: Heart rate and cardiac index |  | $f$ | C | Heart Rate |
|  | BIPLANE CALCULATIONS: |  |  |  |  |
| 9. | Enter data \& calculate ESV \& ESV index |  |  |  |  |
|  | Correction factor, LAO | $\mathrm{CF}_{\text {LAO }}$ | ENTA |  |  |
|  | Systolic area, LAO | SA, cm 2 | ENTA |  |  |
|  | Systolic length, LAO | SL, cm |  | A |  |
|  | Diastolic area, LAO | DA, $\mathrm{cm}^{2}$ | ENTA |  |  |
|  | Diastolic length, LAO | DL, cm | R/S |  | ESV, ESV/m² |
| 10. | Calculate: EDV \& EDV index |  | $f$ | B | EDV,EDV/m² |
| 11. | Calculate: Average systolic \& diastolic DIA. |  | $f$ | D | Sys., Dias. |
| 12. | Calculate: Stroke volume \& stroke index |  | D |  | SV,SI |
| 13. | Calculate: Systolic ejection fraction (\%) |  | E |  | SEF\% |
|  | Calculate: Velocity of circumf. fiber shorteni |  | C |  | $\mathrm{V}_{\mathrm{cf}}$ |
|  |  |  |  |  |  |
|  |  |  |  |  |  |
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| STEP K | KEY ENTRY | KEY Code | comments | STEP KEY | KEY Entry | KEY Code | comments |
| :---: | :---: | :---: | :---: | :---: | :---: | :---: | :---: |
| $0 \cdot 1$ | * Ele ż | 211615 |  | $0 \cdot 5$ |  | -6c |  |
| 062 | 6561 | 2311 |  | 058 | 9 | 69 |  |
| 0 O | 5762 | 3542 |  | 059 |  | -55 |  |
| 064 | Es | 51 |  | 064 | ETH | 24 | Divide by BSA |
| 005 | F+S | 16-51 |  | 061 | *LELE | 2108 | Divide by BSA |
| 066 | ESEI | 2301 |  | 062 | FCle | 3662 |  |
| 040 | ST06 | 35010 |  | 063 | - | -24 |  |
| Q6: | $F \pm S$ | 16-51 |  | 66.4 | F*S | 16-51 |  |
| 009 | STOU | 350 |  | 065 | ST02 | 3542 |  |
| 610 | RTN | 24 |  | 066 | F $\ddagger 5$ | 16-51 |  |
| 611 | RLELI | 2101 |  | 067 | FRTX | -14 |  |
| 012 | CLRG | 16-53 |  | 668 | SPC | 16-11 |  |
| 613 | stoe | 3506 |  | 069 | FTN | 24 |  |
| 014 | RV | -31 |  | 079 | *LELC | 2115 | Calculate $\mathrm{V}_{\text {cf }}$ |
| 015 | 5704 | 35 ט4 |  | 071 | FCl8 | 3608 |  |
| 016 | Kt | -31 |  | 812 | P +5 | 16-51 |  |
| 017 | 5703 | 3503 |  | 873 | FCLE | 3608 |  |
| 018 | R $\downarrow$ | -31 |  | 074 | P +5 | 16-51 |  |
| 619 | ETH | 24 |  | 075 | - | -45 |  |
| 824 | *LELA | 2111 | Calculate ESV, | 076 | CHS | -22 |  |
| 021 | 6589 | 2309 | single plane | 077 | LSTX | 16-63 |  |
| 022 | STOA | 3511 |  | 076 | - | -24 |  |
| 823 | FRTX | -14 |  | 675 | RCL3 | 3603 |  |
| 024 | 6708 | 2288 | $\mathrm{ESV} / \mathrm{m}^{2}$ | 080 | - | -24 |  |
| 025 | *LELE | 2112 | Calculate EDV, | 081 | 6 | 96 |  |
| 026 | $F+5$ | 16-51 | single plane | 082 | - | 09 |  |
| 027 | GSE | 2369 |  | 083 | - | -35 |  |
| 028 | $F+5$ | 16-51 |  | 084 | STac | 3513 |  |
| 0, ${ }^{\text {a }}$ | STOE | 3512 |  | 685 | FRTX | -14 |  |
| [130 | FRTX | -14 |  | use | SFC | 16-11 |  |
| 031 | 6708 | 2208 | EDV/m ${ }^{2}$ | 687 | RTN | 24 |  |
| 032 | *LELG | 2109 | Calculate | 086 | * $2 E L D$ | 2114 | Calculate SV |
| 033 | FCL4 | 3664 | ventricular volumes | 689 | FCLE | 3612 |  |
| 034 | FCLE | 3604 | single plane | 890 | RCLA | 3611 |  |
| 635 | S. | 54 |  | 691 | - | -45 |  |
| 036 | $x$ | -35 |  | 692 | STOL | 3514 |  |
| 637 | 4 | 04 |  | 493 | FRTX | -14 |  |
| 038 | $\times$ | -35 |  | 094 | GT08 | 2248 | Calculate SI |
| 039 | Fi | 16-24 |  | 095 | $\mathrm{F}+\mathrm{S}$ | 16-51 |  |
| 649 | $\bigcirc$ | -24 |  | 696 | 5702 | 3502 |  |
| 64 : | RCLE | 36 ט6 |  | 697 | $F+5$ | 16-51 |  |
| 042 | $\bigcirc$ | -24 |  | 098 | FRTX | -14 |  |
| 043 | 5708 | 35 ¢8 |  | 099 | SPC | 16-11 |  |
| 044 | $\overline{4}$ | 08 |  | 100 | RTN | 24 |  |
| 645 | $x$ | -35 |  | 101 | *LELE | 2115 | Calculate SEF\% |
| 046 | 3 | 03 |  | 102 | RCLLi | 3614 | Calculate SEF\% |
| 047 | $\div$ | -24 |  | 163 | RCLE | 3612 |  |
| 648 | RCL4 | 3604 |  | 104 | $\doteqdot$ | -24 |  |
| 649 | ${ }^{\chi}$ | -35 |  | 105 | EEX | -23 |  |
| 656 | RClu | 3609 |  | 106 | 2 | 02 |  |
| 051 | $\cdots$ | -35 |  | 107 | $\stackrel{x}{\text { P }}$ | -35 |  |
| 652 | - | -62 |  | 168 | FRTX | -14 |  |
| 053 | $\stackrel{8}{8}$ | 98 |  | 109 | STOE | 3515 |  |
| 054 | ${ }^{1}$ | 91 |  | 116 | SPC | 16-11 |  |
| 855 | ${ }^{x}$ | -35 |  | 111 | FTN | 24 |  |
| 656 | 1 | 01 | REGIS | 112 | *LELC | 21613 |  |
| ${ }^{0}{ }^{-} \mathrm{CF}_{\text {RAO }}$ | ${ }^{1}{ }^{C F}$ LAO | $2{ }^{2}$ BSA | ${ }^{3}$ \#Frames ${ }^{4}{ }^{\text {S }}$ RAO | SA RAO | ${ }^{6} \mathrm{SL}_{\text {RAO }}$ | ${ }^{7} \mathrm{SL}$ LAO |  |
| ${ }^{\text {S0 }} \mathrm{CF}_{\text {RAO }}$ | ${ }^{\text {S1 }} \mathrm{CF}_{\text {LAO }}$ | S2 SI |  | ${ }^{55} \mathrm{DA}_{\text {RAO }}$ | ${ }^{\text {s6 }}$ DL RAO | ${ }^{\text {S7 }} \mathrm{LL}_{\text {LAO }}$ | $\frac{S 8}{D}{ }_{D I A} D \cdot D I A^{S 9}{ }^{S 9} D I A_{R A O}$ |
| A ESV |  | B EDV | ${ }^{\text {C }} \quad \mathrm{V}_{\text {cf }}$ | - SV |  | SEF\% | 1 |



# Program Description 



This program has been verified only with respect to the numerical example given in Program Description II. User accepts and uses this program material AT HIS OWN RISK, in reliance solely upon his own inspection of the program material and without reliance upon any representation or description concerning the program material.
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## Program Description II

Sketch(es)

Sample Problem(s) Find 1) stroke volume, cardiac output, cardiac index, 2) mean arterial pressure, total systemic resistance (units dyne sec $\mathrm{cm}^{-5}$ ), systemic vascular resistance (units, dyne sec $\mathrm{cm}^{-5}$ ), 3) total pulmonary resistance, pulmonary vascular resistance

Height 5'7" Weight 69.4 kg
BSA $1.81 \mathrm{~m}^{2}$

| $d Z / d t$ | $=.81$ | BP systemic $=120 / 80 \mathrm{mmHg}$ |
| :---: | :--- | :--- |
| T | $=.23$ | CVP $^{2}\left(\overline{\mathrm{P}}_{\text {RA }}\right)=15 \mathrm{mmHg}$ |
| L | $=28.5$ | $B P$ pulmonary $=44 / 24 \mathrm{mmHg}$ |
| $Z_{0}$ | $=20.2$ | $\bar{P}_{\text {LA }}$ |

Heart Rate $=103$

Solution(s) $[f][E] \cdots-\cdots 1.00[f][E] \cdots 0.00$ (set for calc by $C O$ )

1) 1.81 [f][D] . $81[\mathrm{ENTA}]$.23[A] $28.5[\mathrm{~B}] 20.2[\mathrm{C}]---->50.06 \mathrm{ml}, \mathrm{SV} ; 103[\mathrm{D}]--->5.161 / \mathrm{mi}$
2) 120 [ENT $\uparrow$ ] $80[\mathrm{f}]$ [A] $\ldots-->93.33 \mathrm{mmHg}$, mean press 18.10 units, total sys. resist.
[R/S]------>1447.96dyne-sec-cm ${ }^{-5}$, sys. resist.
15[f] [B] -----> 15.19 units, sys. vasc. resist.
[R/S]------>1215.25 dyne-sec-cm ${ }^{-5}$, vasc. resist.
3) $44[E N T \uparrow] 24[f][A] \ldots--->30.67 \mathrm{mmHg}$, mean pulm. press. 5.95 units, total pulm. resist. 13[f][B] ------> 3.43_units, pulm, vasc resist.
Reference(s) Pomerantz, M., Delgado, F., and Eiseman, B.: Unsuspected Depressed Cardiac Output Following Blunt Thoracic or Abdominal Trauma. Surg. 70:865-871, 197 Blackwell Scientific Publications: Medical and Surgical Cardiology, pp. 120-121, Wm. Cowles \& Sons, Ltd., London, 1969. Kubicek, William: The Minnesota Impedance Cardiograph; Theory and Application. Biomed. Eng., Vol. 9, No.9, Sept.1974,pg.410-42)

IMP. CARD OUTPUT, SYS \& PULM. RESIST.
TOTAL RES. VASC RES.
BSA CO or CI $d Z / d t \uparrow T$
$L \quad Z_{0} \rightarrow S V$ RATE $\rightarrow$ C0



## Program Description

| Program Title BASIC EKG DETERMINATIONS |  |
| :--- | :--- | :--- |
| Contributor's Name Hewlett - Packard Company |  |
| Address 1000 N. E. Circle Boulevard   <br> City Corvallis State Oregon |  |

Program Description, Equations, Variables
Given the magnitudes of both the positive and negative deflections of leads I and III (in millimeters of a graduated EKG)
displayed is the predicted magnitude (pos. minus neg. deflections) according to Einthoven's Law: Lead II = Lead I + Lead III of Lead II
computed is the mean electric axis of the heart
axis rectangular coordinates $=$ Lead $I(.5774)+$ Lead III(1.1547) axis angular coordinates $=$ conversion to polar coordinates

Given either the heart rate or the $R-R$ interval, the other is computed
heart rate $=\frac{60}{R-R \text { interval }}$
computed is the predicted normal $Q-T$ interval for that rate

$$
\mathrm{Q}-\mathrm{T}=0.39 \quad \mathrm{R}-\mathrm{R} \pm .04
$$

## Operating Limits and Warnings

Both positive and negative deflections must be entered for each lead

## Program Description II



Sample Problem(s)
Given the data as represented above in the graph:

$$
\begin{array}{ll}
\mathrm{I}^{+}=3.0 \mathrm{~mm}(\mathrm{mv} * .1) & \mathrm{III}^{+}=2.5 \mathrm{~mm} \\
\mathrm{I}^{-}=1.0 \mathrm{~mm} & \mathrm{III}^{-}=1.5 \mathrm{~mm}
\end{array}
$$

Heart rate $=75 \mathrm{bpm}$

Find the expected magnitude of lead II, the axis deviation in degrees (of the mean electric axis), the mean axis magnitude, the $R-R$ interval, and the calculated $Q-T c$ interval.

Solution(s) 3 [ENTY] 1 [A] 2.5 [ENT $\uparrow$ ] 1.5 [B] $\rightarrow 3.0$ Lead II
$[\mathrm{C}] \rightarrow-8^{\circ}$ (left axis deviation - slight)
$[R / S] \rightarrow 3.1$ mean axis magnitude
75 [D] $\rightarrow 0.80 \mathrm{sec} ., R-R$ interval
(optional) $0.80[\mathrm{D}] \rightarrow 75$, heart rate
[E] $\rightarrow 0.35 \mathrm{sec}, \mathrm{Q}-\mathrm{Tc}$ interval

## Reference (s)

Schaub, Frank A., Fundamentals of Clinical Electrocardiography, pgs. 15, 23-26, Geigy Pharmaceuticals, New York, 1966.

This program is a translation of the HP-65 Users' Library Program \# 00455A submitted by Steven A. Conrad.


| STEP | INSTRUCTIONS | INPUT <br> OATA/UNITS |  | KEYS |
| :---: | :---: | :---: | :---: | :---: |
| DATA/UNITS |  |  |  |  | (



NOTES

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Medical Practitioner<br>Anesthesia<br>Cardiac<br>Pulmonary<br>Chemistry<br>Optics<br>Physics<br>Earth Sciences<br>Energy Conservation<br>Space Science<br>Biology<br>Games<br>Games of Chance<br>Aircraft Operation<br>Avigation Calendars<br>Photo Dark Room<br>COGO-Surveying<br>Astrology<br>Forestry

## CARDIAC

A group of programs for carrying out common cardiac catheterization laboratory calculations. A number of the programs are designed to be self consistent for sequential use. Ventricular function calculations from radiographic data and basic EKG determinations are included.

CARDIAC PROGRAM SERIES
VIRTUAL $\mathrm{PO}_{2}$ AND $\mathrm{O}_{2}$ SATURATION AND CONTENT
BODY SURFACE AREA FOR CARDIO PULMONARY PROGRAMS
dYE CURVE CARDIAC OUTPUT
FICK CARDIAC OUTPUT
VALVE AREA
ANATOMIC SHUNTS
CONTRACTILITY
STROKE WORK
EJECTION-FRACTION, EJECTED-VOLUME, CARDIAC OUTPUT
CALCULATIONS OF LEFT VENTRICULAR FUNCTIONS FROM ANGIOGRAPHS
IMPEDANCE CARDIAC OUTPUT, SYSTEMIC AND PULMONARY RESISTANCE
BASIC EKG DETERMINATIONS


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